

# WALL SHEAR STRESS TOPOLOGICAL SKELETON VARIABILITY PREDICTS PLAQUE PROGRESSION IN HUMAN CORONARY ARTERIES

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## Introduction

Although low wall shear stress (WSS) has become the consensus hemodynamic mechanism for coronary atherosclerosis, the exact biomechanical stimulus affecting atherosclerosis evolution is still undetermined [1]. Aiming at bridging this gap of knowledge, recently the WSS topological skeleton (TS) is receiving increasing interest, because of (1) its link with flow features associated with vascular dysfunction [2], and (2) its capability to concur to the description of the complex biomechanical stimulus affecting atherosclerosis evolution [3]. Briefly, the WSS TS is composed by fixed points, where the WSS vanishes, and unstable/stable manifolds connecting them, where WSS exerts a contraction/expansion action on the endothelium [4]. Here we test the ability of WSS TS, solely or synergistically with plaque phenotypes, to predict the temporal evolution of coronary artery plaque atheroma volume (PAV), a hallmark of atherosclerosis development, in 38 patient-specific computational models of human coronary arteries.

## Methods

A non-culprit coronary segment for 37 hemodynamically stable patients was imaged at baseline (T1) and at 1 year follow-up (T2). Vessel geometries were reconstructed at T1, and computational hemodynamic simulations were carried out prescribing patient-specific boundary conditions. Widely adopted descriptors of WSS magnitude and multidirectionality were tested (i.e., TAWSS, OSI, RRT, and transWSS). Additionally, a Eulerian method was applied to analyse the WSS TS [4], identifying WSS contraction/expansion regions at the coronary luminal surface by the divergence of normalized WSS vector field ( $DIV_{WSS}$ ). The amount of variation in WSS contraction/expansion action along the cardiac cycle T was quantified by the Topological Shear Variation Index (TSVI) [2]:

$$TSVI = \left\{ \frac{1}{T} \int_0^T [DIV_{WSS} - \overline{DIV_{WSS}}]^2 dt \right\}^{1/2} \quad (1)$$

Plaque progression was evaluated as the difference between PAV measurements ( $100 \times \text{plaque volume} / \text{total vessel volume}$ ) at T2 and T1 averaged over  $3\text{mm}/45^\circ$  luminal sectors. Additionally each sector was classified as lipid rich, fibrous or plaque free based on OCT images. Hemodynamic descriptors were averaged over  $3\text{mm}/45^\circ$  luminal sectors and divided into artery-specific low, mid and high tertiles to perform a statistical analysis on the associated  $\Delta PAV$ , solely or in combination with plaque phenotype.

## Results

The luminal distribution of TAWSS, TSVI and  $\Delta PAV$  are reported in Figure 1A for an explanatory case. Overall, sectors exposed to high TSVI at T1 exhibited  $\Delta PAV$  in the T2-T1 time interval significantly higher than sectors exposed to low or mid TSVI at T1 (figure 1B). A clear trend emerged also for the exposure to low TAWSS at T1 and high  $\Delta PAV$ . Plaque phenotype acted synergistically with TAWSS or TSVI regarding plaque progression: at low TAWSS or high TSVI sectors in combination with lipid rich plaque,  $\Delta PAV$  values were significantly higher ( $p < 0.01$ ) than expected based on the individual contribution of hemodynamics. Low values emerged for OSI ( $< 0.01$ ) and transWSS ( $< 0.15\text{Pa}$ ) suggesting a minor role of WSS multidirectionality in promoting aggravating biological events.

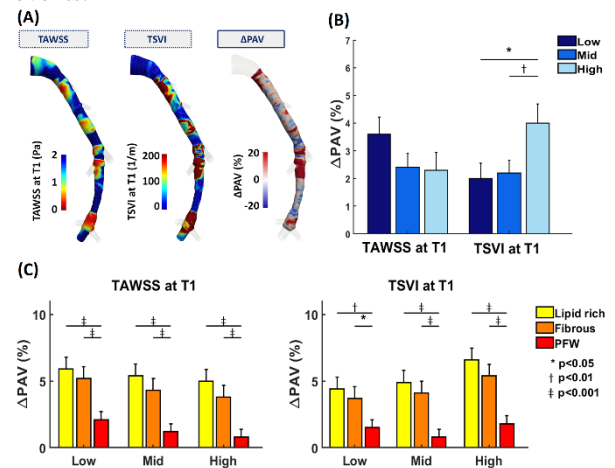


Figure 1: (A) TAWSS, TSVI and  $\Delta PAV$  luminal maps; (B) TAWSS and TSVI vs. estimated PAV: (B) solely; (C) in combination with OCT-derived plaque phenotypes.

## Discussion

Here we demonstrate that luminal exposure to high TSVI, solely or combined with lipid rich plaque phenotype, was associated with plaque progression. Physically, TSVI quantifies WSS contraction/expansion action variability on the endothelium, describing a different hemodynamic stimulus with respect to low TAWSS. This study confirms recent findings on TSVI as biomechanical marker of vascular disease, encouraging further trials for its translation to clinics.

## References

1. Brown AJ et al., Nat Rev Cardiol, 13:210-220, 2016.
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4. Mazzi V et al., Biomech Model Mec, 19(5):1403-23, 2020.

